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assessment of suspected postoperative patient–prosthesis mismatch. We recently reported our experience with the modality of cine-computed tomography (CT) imaging, essentially moving pictures of the valve in motion.² This technique allows unprecedented precision in imaging the valve and its leaflet motion. The cine-CT gives the sensation of almost "being there," inside the heart, watching the valve work in real time (Figure 2 and Video 1). Cine-CT easily detects thrombus, pannus, and restricted leaflet motion with great accuracy and resolution. In our recent report, we found that many cases of late-onset suspected patient–prosthesis mismatch could be traced to an increase in a patient's weight over years postimplant, placing an increased circulatory burden on a properly functioning valve.

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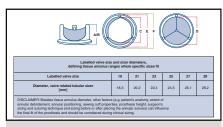
Commentary: Valve Labeling Task Force: Efforts now needed by manufacturers and surgeons

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Now that the 2 position articles of the European Association for Cardio-Thoracic Surgery, American Association for Thoracic Surgery, Society of Thoracic Surgeons Task Force on Valve Labeling have been published, ^{1,2} we find ourselves on the threshold of reaping the benefits of these extensive deliberations. However, we are in the red zone but not across the goal line.

The focus of the joint American Association for Thoracic Surgery, European Association for Cardio-Thoracic Surgery, Society of Thoracic Surgeons Valve Labeling Task Force has been on uniformity of labeling with regard to dimensions, size, and hemodynamic performance. This

0022-5223/\$36.00



Recommended "Valve Chart." Distillate of the work of the Valve Labeling Task Force.

CENTRAL MESSAGE

Implementation of the Task Force on Valve Labeling recommendations will require buy-in by manufacturers and familiarization with the data tables by surgeons.

second follow-up article² lays out the outcomes and decisions of the task force that will further aid surgeons in optimal valve selection with a clear elucidation of valve dimensions and hemodynamic performance.

Two further steps are needed before benefits of these efforts translate to surgeons and their patients.

 Guideline implementation. The manufacturers of prosthetic heart valves need to buy-in to the concept of complete, frank, evidence-based labels for each type and size of valve. They not only need to adopt the recommended table but also need to fill in the data. This will include not only easily measured (now standardized) physical dimension data but also not so easy accurate, echocardiography-based assessments of functional valve

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Disclosures: J.A.E.: Principal, CoolSpine; Consultant for CryoLife; Data/Safety Monitoring Board for Terumo. P.A. reported no conflicts of interest.

The *Journal* policy requires editors and reviewers to disclose conflicts of interest and to decline handling or reviewing manuscripts for which they may have a conflict of interest. The editors and reviewers of this article have no conflicts of interest.

Received for publication Oct 16, 2020; revisions received Nov 2, 2020; accepted for publication Nov 13, 2020; available ahead of print Nov 19, 2020.

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J Thorac Cardiovasc Surg 2021;161:562-4

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AO	RTIC		Valve chart for "VALVE" by "MANUFACTURER"															This chart is developed according to the standardized criteria of the EACTS-STS-AATS Valve Labelling Task Force					
	Probability of severe* Prosthesis-Patient Mismatch														Possible implant positions								
	"MANUFACTURER" - "VALVE MODEL"																						
Labelled valve size		19		21		23		25		27		29											
															Physical dimensions								
Patient BMI [kg/m ²]		< 30	≥ 30	< 30	≥ 30	< 30	≥ 30	< 30	≥ 30	< 30	≥ 30	< 30	≥ 30	Labelled valve size	Overall profile height	Outflow profile height	Minimum internal diameter	Interr sten diame	nt eter	External stent diameter	sewir diar	ternal ng ring meter	
Patient BSA [m ²]	1,2	9%	3%	7%	4%	4%	3%	2%	1%	1%	1%	0%	0%		[mm]	[mm]	[mm]	[mm	·	[mm]	<u> </u>	nm]	
	1,3	16% 25%	7% 12%	12% 18%	7% 10%	7% 11%	4% 7%	3% 6%	2% 3%	2% 3%	1% 2%	0% 0%	0%		(A)	(B)	(C)	(D)		(E)	((F)	
	1,4	25% 34%	12%	24%	10%	11%	10%	6% 8%	3% 5%	3% 5%	3%	0%	0%	19	13	13	17,1	18		19,2	1 :	24	
	1,5	43%	25%	29%	19%	19%	13%	12%	8%	7%	5%	0%	0%	21	14	14	19,2	20		21,2		26	
	1,7	51%	31%	35%	24%	23%	16%	15%	10%	10%	7%	0%	0%	23	15	15	21.2	22		23.2		28	
	1,8	58%	38%	40%	28%	28%	20%	19%	13%	13%	9%	0%	0%				,				+		
	1,9	64%	44%	45%	33%	32%	23%	23%	16%	15%	11%	0%	0%	25	16	16	23,2	24		25,3		30	
	2,0	69% 74%	50% 55%	50%	37% 41%	35% 39%	27% 30%	27% 30%	19% 22%	18% 21%	14% 16%	1%	0%	27	17	17	25,2	26		27,3		32	
	2,1	74%	55% 60%	54% 58%	41%	39% 42%	30%	30%	22%	21%	16%	1% 2%	0% 1%	29	18	18	27,2	28		29,3	:	34	
	2,2	80%	64%	61%	48%	45%	36%	37%	28%	27%	21%	3%	1%										
	2,4	83%	68%	64%	51%	48%	39%	40%	31%	30%	23%	4%	2%										
Study details	2,5 EOA, mean ± SD [cm ²]	85% 1,1 ±	71% 0,2	67% 1,3 ±	54% 0,3	51% 1,6 ±	41% 0,4	43% 1,8 ±	34% 0,4	32% 2,2 ±	25% 0,5	6% 2,8 ±	3% : 0,3										
	Patients per valve size (n) Prospective	25 yes			52 yes		79 yes		65 Ves		43 Ves		2 S										
	Centers per valve size (n)		3		3		3		3		3			1									
	Pooled data	no		n	no		no		no		no		c c		Labelled valve size and sizer diameters,								
	Regulatory	no		n	no		no		no		no		c	defining tissue annulus ranges where specific sizes fit									
	Echo core lab	yes		ye	yes		yes		yes		yes		s	Labelled valve size		19	21	23	25	27	29		
	Period of data collection	2012 - 2014		2012 -	2012 - 2014		2012 - 2014		2012 - 2014		2012 - 2014		2014	Diame	ter, valve relate [mm]	18,3	20,2	22,4	24,5	26,1	28,2		
	Timing of postop echo	3 moi	3 months		3 months		3 months		3 months		3 months		nths		DISCLAIMER: Besides tissue annulus diameter, other factors (e.g. patient's anatomy, extent of								
COLOR CO	M is defined as iE DING: yellow india A is below the sev	cates that	the perce	ntage pro										annular debridement, annular positioning, sewing culf properties, prosthesis heipht, surgeon's sizing and suturing technique and sizing before or after placing the annular sutures) can influence the final fit of the prosthesis and should be considered during clinical sizing.									
DISCLAIME	R: This chart is a cular valve, but the	support to	ol to estir	nate the p								replacem	ient					v	ersion nu	mber v1, iss	ue data 01	1-01-2020	

FIGURE 1. Standardized valve chart for aortic valves, which provides essential information on surgical heart valve characteristics in a uniform manner and allows for comparability between different surgical heart valve models without demanding radical changes in current surgical heart valve designs or labeling. *BMI*, Body mass index; *BSA*, body surface index; *PPM*, patient–prosthesis mismatch. Reprinted with permission from Durko and colleagues.²

size and anticipated gradients for each size valve and particular patient. In most cases, the manufacturers will have adequate data on hand. The task force has called for a minimum of 30 Doppler echocardiograms providing in vivo human data on mean transprosthetic gradient and effective orifice area for each valve in every size. The task force has further stipulated that these data must be accrued within 30 days and 1 year after implantation. If such information is not already available, additional clinical studies will be required of the manufacturer. Furthermore, the manufacturer must include in the charts a patient–prosthesis mismatch (PPM) calculating nomogram. This plots the likelihood of PPM for the proposed valve for each patient's body surface area (Figure 1).

2. Surgeon use. The charts are designed for both completeness and ease of use. The surgeon finds the chart (externally available on the boxes and in paper and computer information sheets) for the valve he is considering. He plots the valve size along the upper horizontal axis and the patient's body surface area along the left vertical axis. The color code lets the surgeon know the likelihood of severe PPM. A yellow color indicates a 50% or greater likelihood of PPM. The surgeon can modify his valve choice accordingly. The accompanying schematic diagram shows the prosthetic valve in position, with the physical dimensions of the valve indicated.

Cardiac surgeons and manufacturers generally have a positive and strong relationship because they have the shared goals of patient perioperative safety, long-term survival, and good symptomatic state. We anticipate enthusiastic "buy-in" from the manufacturers for this novel approach, especially because they had vocal seats at the table during the task force discussions and expressed full engagement in the goals and plans, in many cases helping us determine feasible approaches to maximize an educated decision on valve choice for our patients. We hope that surgeons find ease and reassurance in using these new tools.

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